Self-Motion Processing in Humans from Psychophysics to High Density Electrical Mapping

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#### Talk Overview

- Passive Heading detection
  - 1. Cue Conflict
  - 2. Neural correlates of heading detection change
- Active tasks
  - 3. Feasibility of neural recordings while walking
  - 4. Cognitive flexibility while walking in young and old

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## Self-motion

- Self-motion
  - Walking
  - Driving
- Cues for Self-motion
  - Visual
  - Vestibular
  - Somatosensory
  - Etc.





# Inertial (vestibular)

- Otholiths
  - Linear acceleration
- Semi-circular Canals
  - Rotational velocity
- Function
  - Eye movements
  - Heading
- Disorders
  - Vertigo
  - Motion sickness
  - Falls



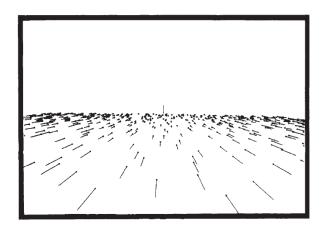
# Optic flow

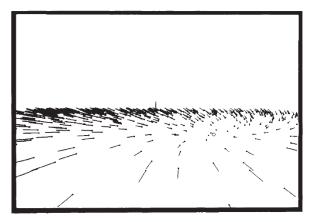
#### Behavioural

- Relative distance perception
- Heading

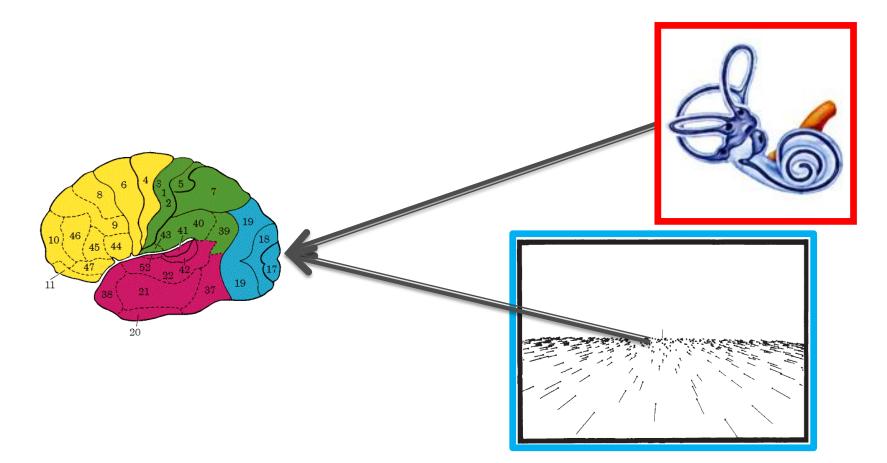
#### Neurophysiology

- Vection
  - hFMRI (MT+)
- Heading
  - MST



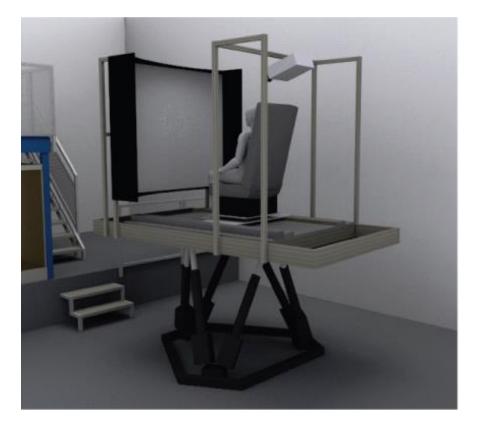


#### **Combination of Senses**





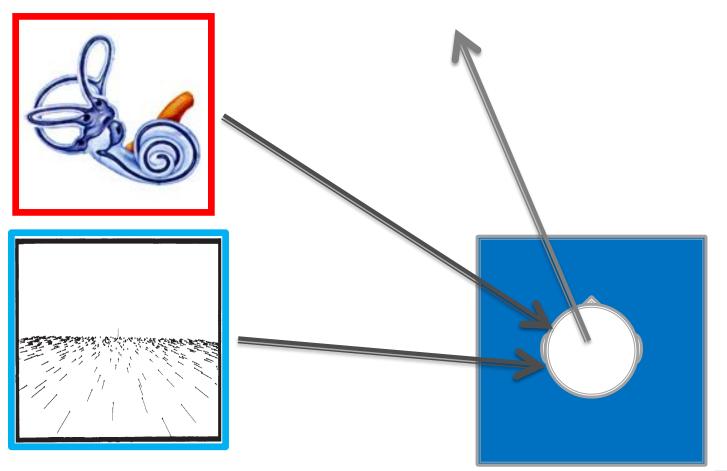
# Virtual reality setup and stimuli





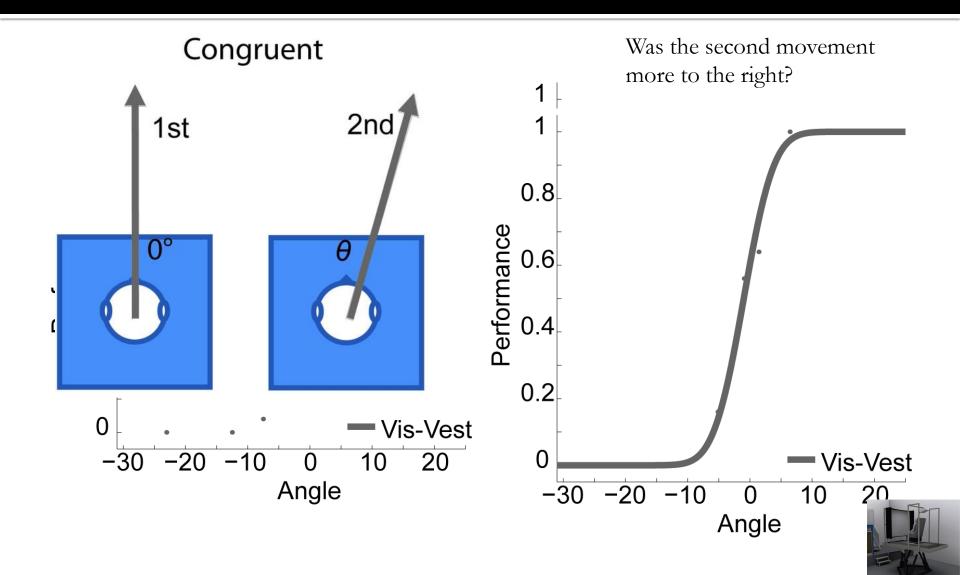


#### Visual-Vestibular Integration for Heading

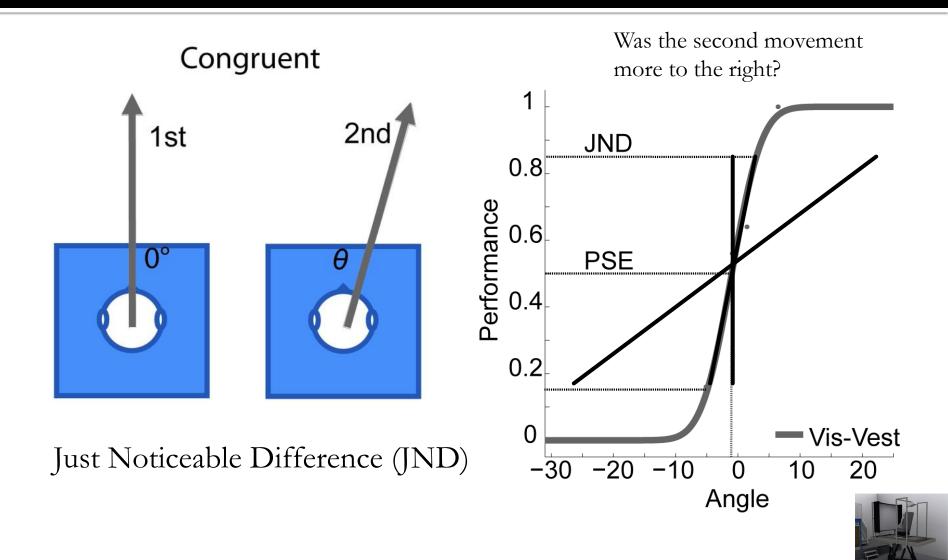




# Reliability

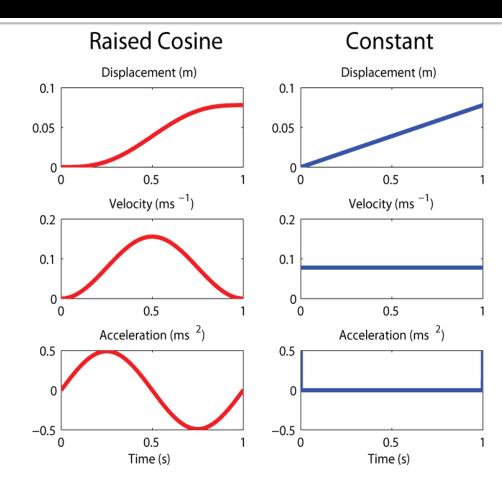


# Reliability



# **Information Conflict**

- Conditions
  - Visual
    - Raised cosine
    - Constant velocity
  - Vestibular
    - Raised cosine
  - Visual-vestibular
    - Raised cosine velocity
    - Constant velocity (conflict)

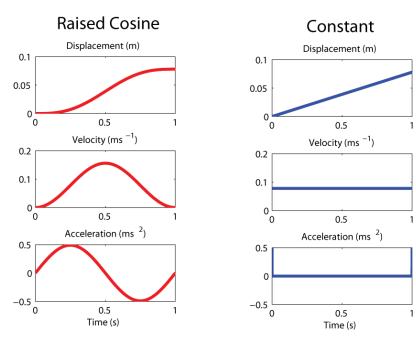




# Visual motion Profile and heading estimation

#### **Objective**

To investigate if the velocity and acceleration play a role in visual heading discrimination



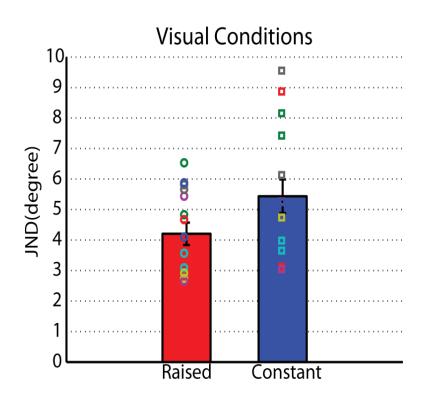
#### **PREDICTION 1**

The constant velocity profile will give more reliable results as it is highly predictable

#### **PREDICTION 2**

The more "natural" raised cosine profile is more reliably as we are more commonly exposed to it

#### Results

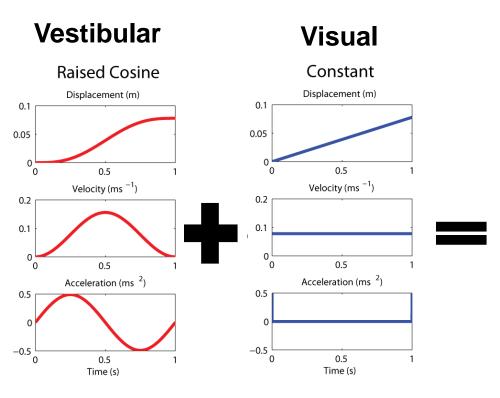


The raised cosine profile is gives more reliable estimates of visual heading

#### **Predictions for the discrepant condition**

#### **Objective**

To investigate the combination of visual and vestibular information under different visual motion profile conditions



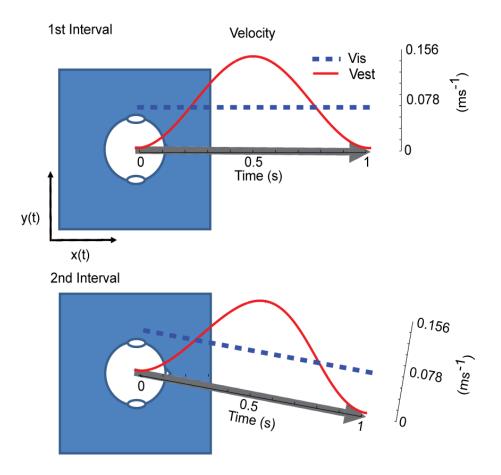
#### **PREDICTION 1**

The visual and vestibular information do not combine in an optimal fashion

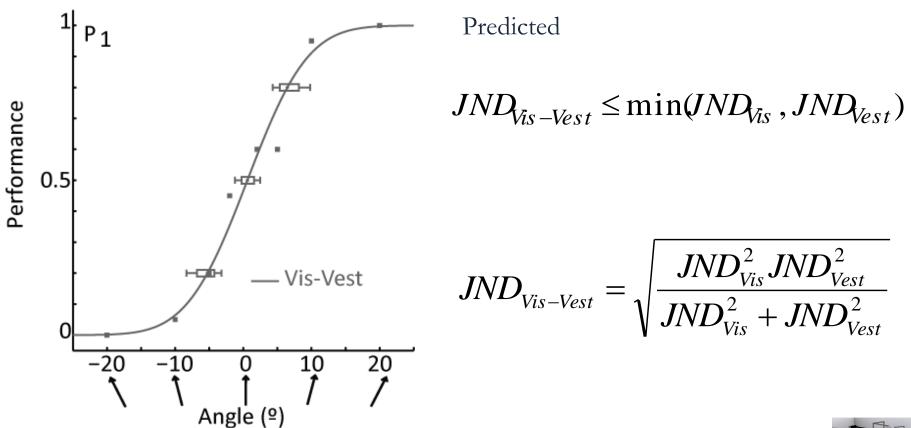
#### **PREDICTION 2**

Combination of senses is not dependent on the motion profile

# Effect of visual motion profile on heading discrimination

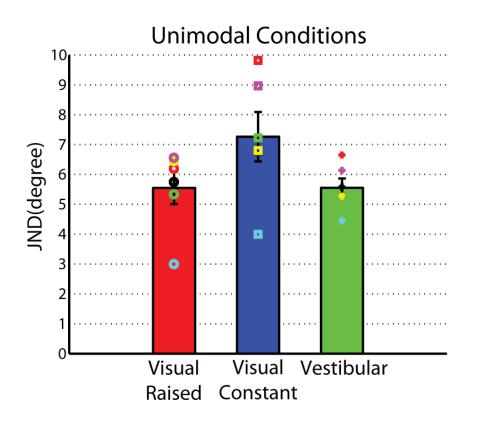


#### **Combination of Senses**



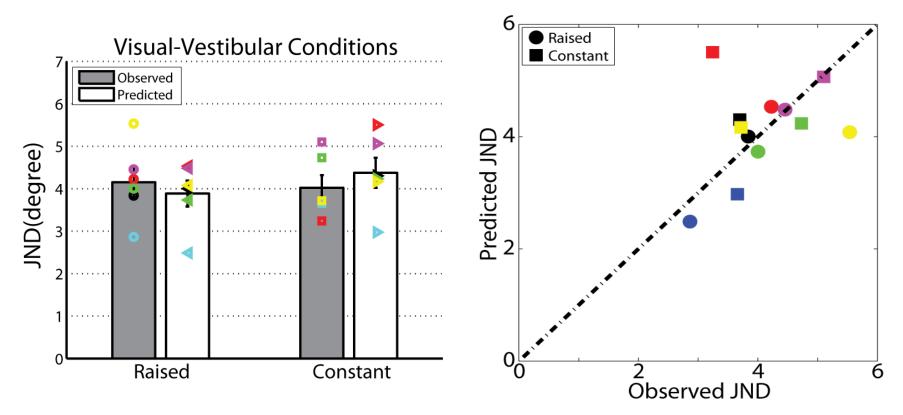


#### Unimodal results





### **Multisensory Results**





## Conclusion

- Visual motion is not just a snap shot but an accumulation of information
  - The more natural profile yielded the more accurate heading discrimination
- Visual and Vestibular cues combine in an optimal fashion even when there is an information conflict

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#### Neuronal Correlates of Self-Motion

- Behavioural tasks
  - Open loop
  - Closed loop
- Imaging techniques
  - fMRI
  - MEG
  - TMS
  - Imaging in non-human primates



# Benefits of using EEG

- Systems level snapshot
- Attention deployment
- Temporal resolution
- Light weight
- Real world environment
- Online feedback loop



# The cusp of a wave

#### HARDWARE

 Advances in motion platform design

 Advances in electrodes design

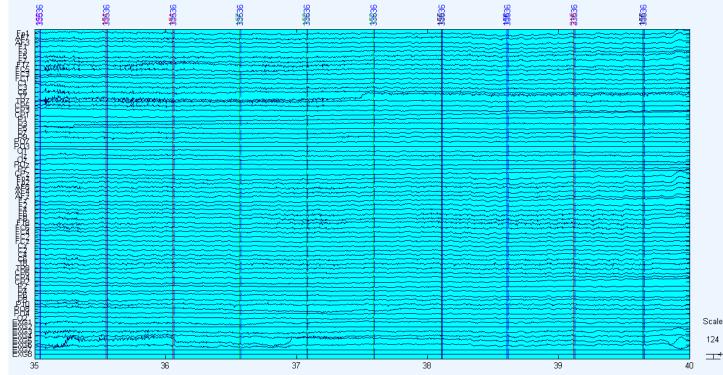
#### SOFTWARE

- Advanced analysis techniques
  - Independent Component Analysis
  - Source localisation techniques
  - Mobile Brain Imaging (MoBi – Scott Makeig)
- Individual data analysis
  - Bootstrapped Statistics



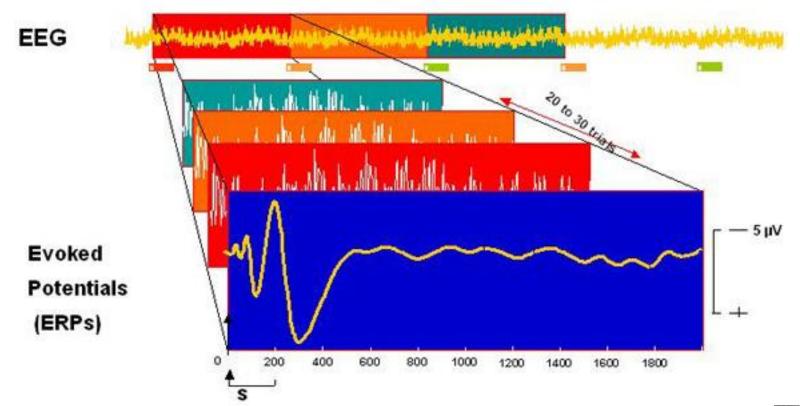
# Electroencephalography (EEG)





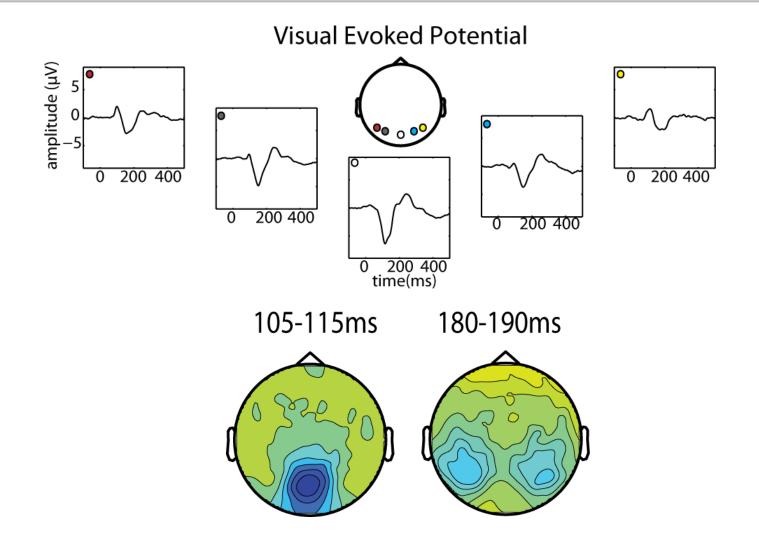


# **Event-Related Potential (ERPs)**





# Electroencephalography (EEG)





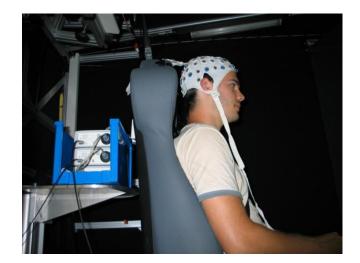
#### EEG on a Stewart Platform

#### Experiment I

EEG on the platform

#### Experiment II

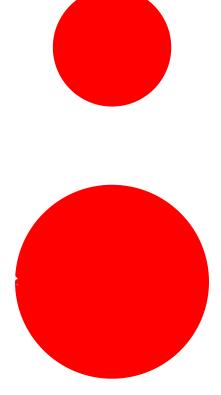
Vestibular P3





#### **Control experiment**

- Can we get an EEG signal while moving people?
- Visual P3 paradigm
  - 80% Standard
  - 20% Target
- Four levels of motion
  - Stationary
  - Idle
  - Slow 0.5 hrtz at 0.25mG
  - Fast 0.5 hrtz at 0.75mG

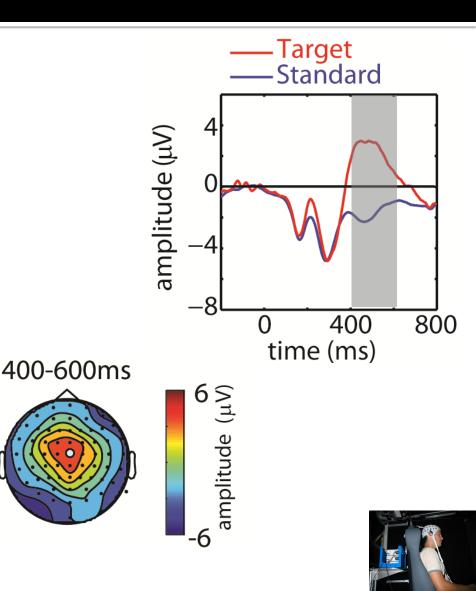




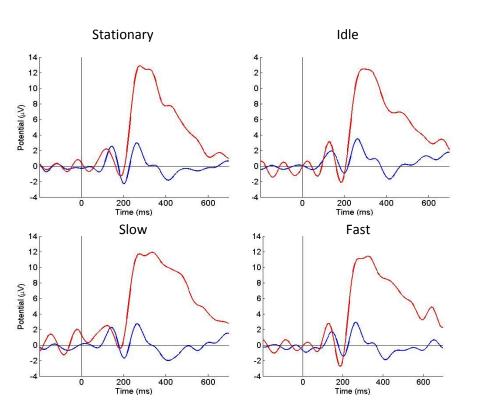
# The Oddball Paradigm

- Change detection is essential to interact with our environment
- Robust response elicited for visual, auditory, somatosensory and olfactory stimuli

#### SSSTSSSSTSSSTSST



# **Results - Control Experiment**



#### Summary

• We can conduct EEG on the motion platform

IEEE Neural Eng (2009)

Nolan, Whelan, Foxe, Bulthoff, Reilly, Butler

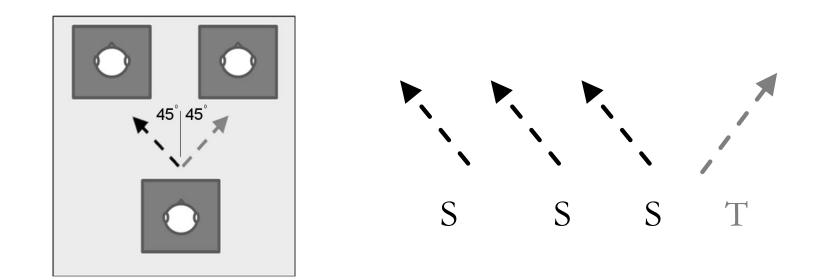
# Vestibular Oddball

- Vestibular Conditions
  - Diagonal Left Target
  - Diagonal Right Target
- Vestibular P3 paradigm
  - 80% Standard (320 sweeps)
  - 20% Target (80 sweeps)
- 15 participants
- 128 scalp channels





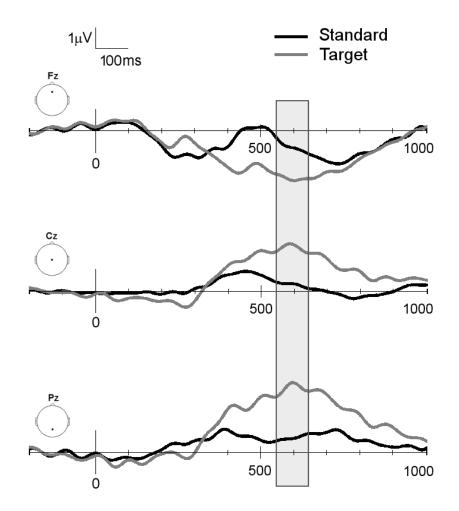
#### Procedure



#### A neuronal marker for vestibular change detection



#### Results- Vestibular P3

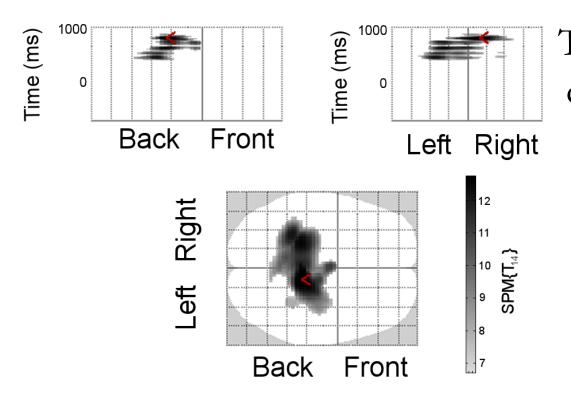


 Statistical difference between the standard and target



# P3 distribution

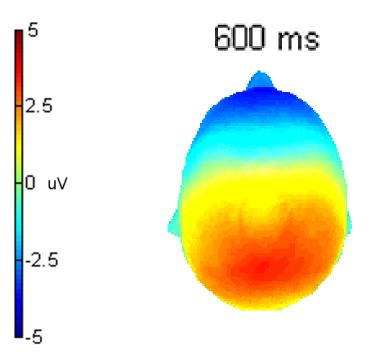
#### **Target vs Standard**



Target topographic scalp distribution is similar to the typical P3 distribution for other sensory modalities



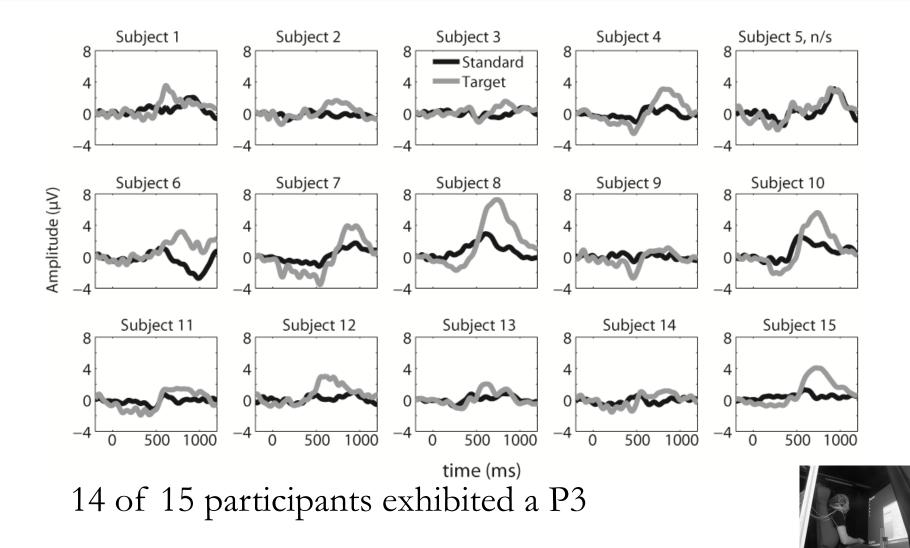
# **Scalp Distribution**



 Target topographic scalp distribution is similar to the typical P3 distribution for other sensory modalities



# Individual Participant data



#### Summary



This is the first time vestibular heading change detection has been shown to elicit a P3 component.

Experimental Brain Research 2012

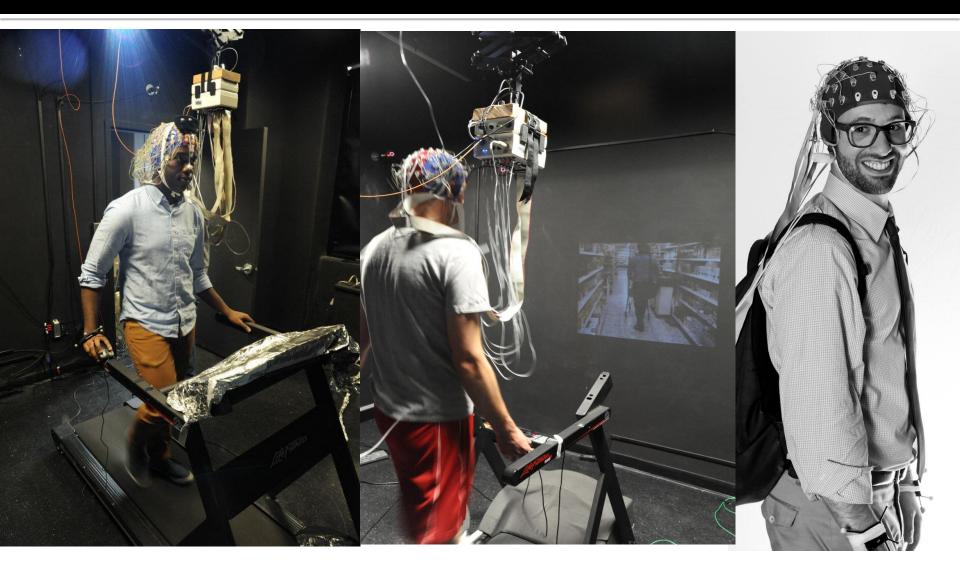
Nolan, Butler, Whelan, Foxe, Bulthoff, Reilly

#### Talk Overview

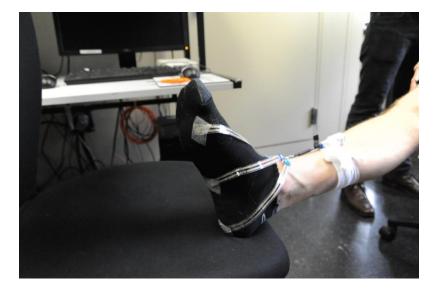
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# EEG while Walking



#### EEG while Walking



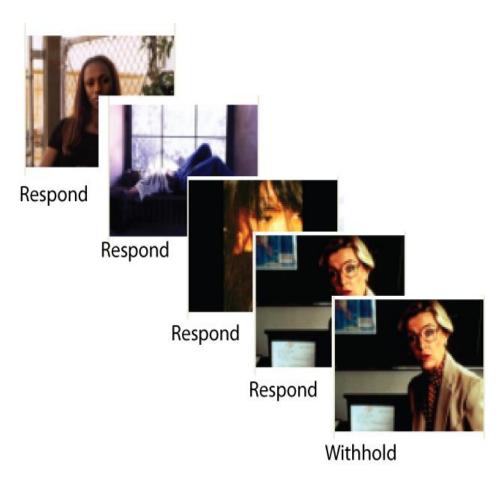


#### EEG while Walking





# **Response Inhibition Task**



#### Task

- Go/Nogo Response Inhibition Task
- NoGo: repetition of the same picture
- Stimulus presentation rate 1/per sec
- Go/Nogo = 80/20%
- Conditions
  - Sitting
  - Walking Slow (2.4 km/h)
  - Walking Fast (5 km/h)



# **Response Inhibition Task**

#### • Hit:

- correct response in a go trial
- Correct Rejection:
  - successful withholding of a response in a nogo trial
- False Alarm:
  - Executing a response in a nogo trial

Feasible to acquire usable EEG data while walking
 Interaction of walking and response inhibition



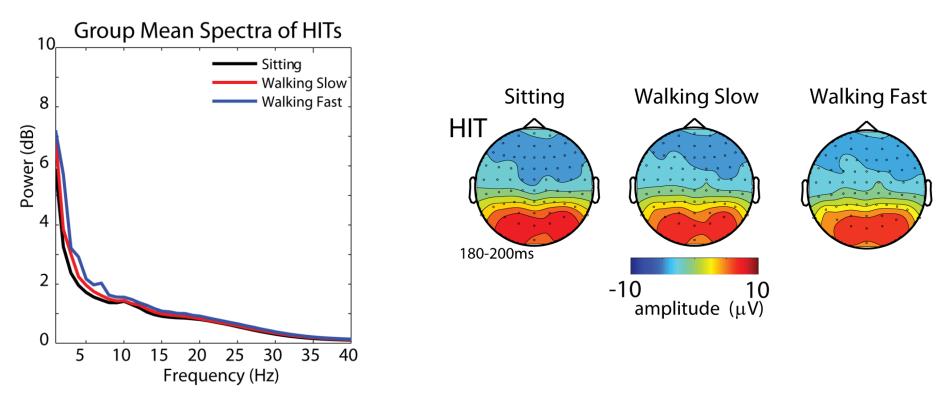
## **Behavioral and SNR Results**



	Sitting	Walking	g Walking	p-value
		Slow	Fast	
RT in msec	399.1	408.2	401.2	0.53
Hit in %	96.4	98.3	98.5	0.49
CR in %	68.6	70.4	69.4	0.6
	Sitting		Walking	Walking
			Slow	Fast

		310W	Γαδι
SNR Hit (dB)	54.8±2.3	53.6±1.6	49.9±2.2
SNR CR (dB)	35.3±2.0	34.0±2.5	32.6±2.2

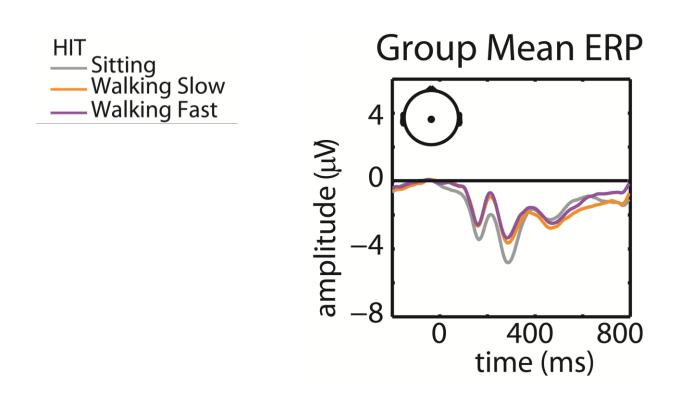
#### Results



Highly similar early evoked response and power spectrum point to the feasibility of acquiring EEG while walking



#### Results



34th Annual International Conference of the IEEE EMBS San Diego, California USA, 28 August - 1 September, 2012

Pierfilippo De Sanctis, John S. Butler, Jason M. Green, Adam C. Snyder, and John J. Foxe

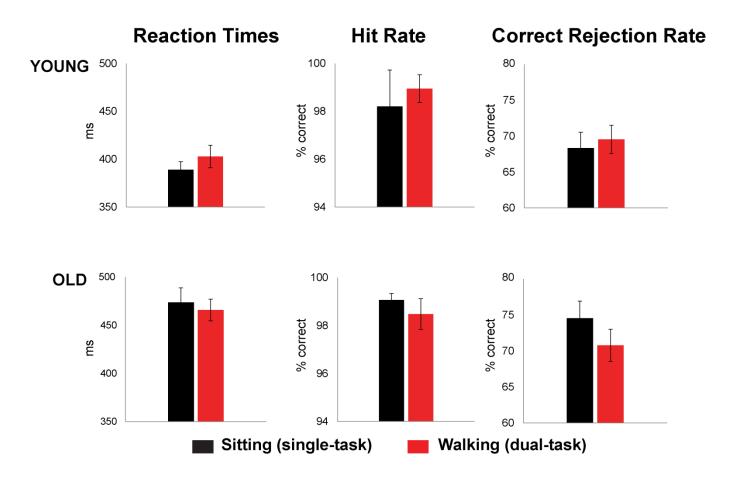
The aging brain shows less flexible reallocation of cognitive resources during dual-task walking: a mobile brain/body imaging (MoBI) study

Age	Young	Old
Range	21.8-36.1	57.7-71.0
Mean	27.2	63.9
SD	4.6	4.0



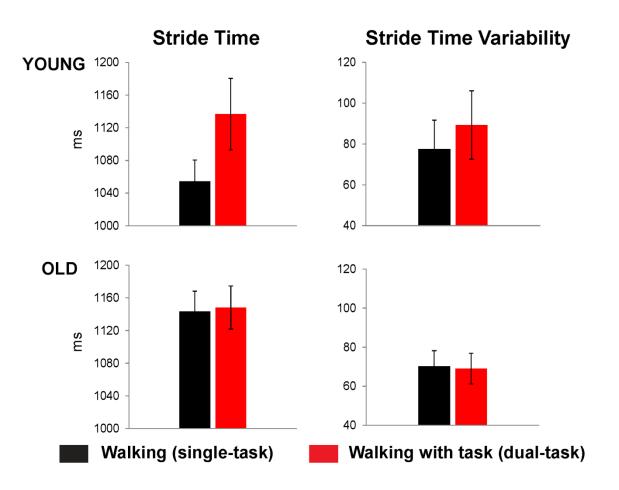


#### Behavioural



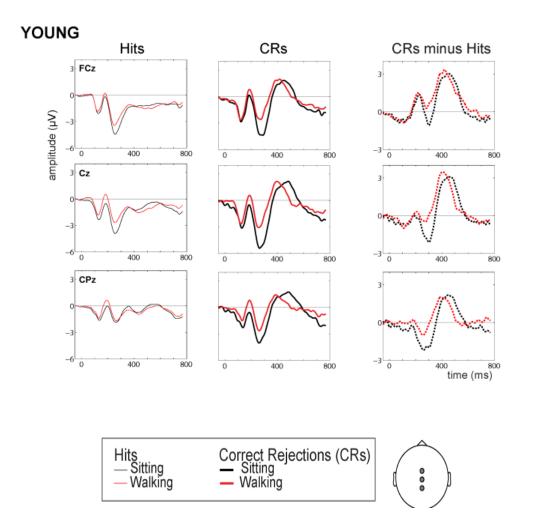


#### **Gait Parameters**



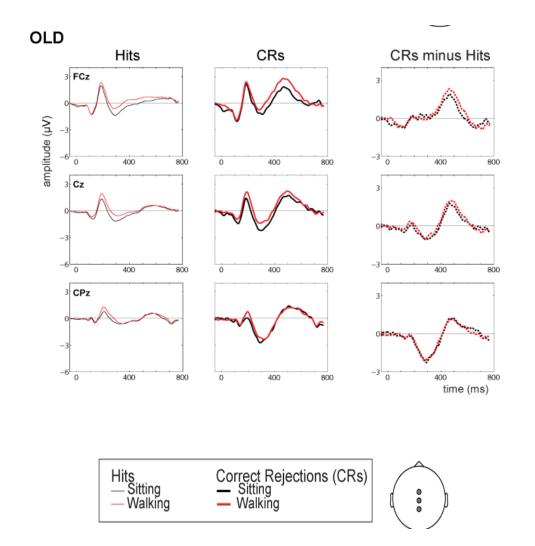


# ERP - Young



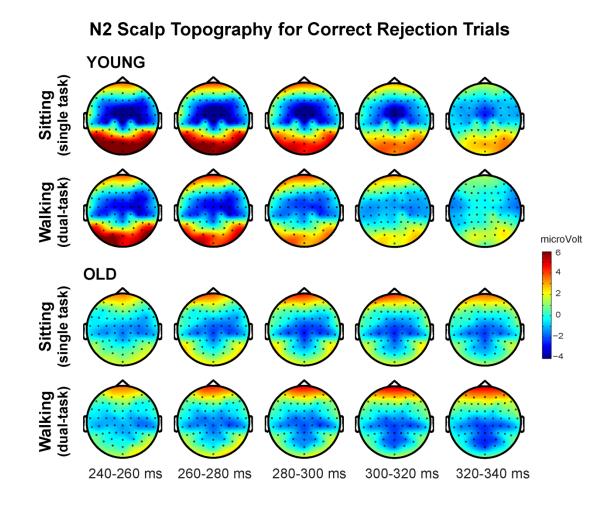


### ERP - Old



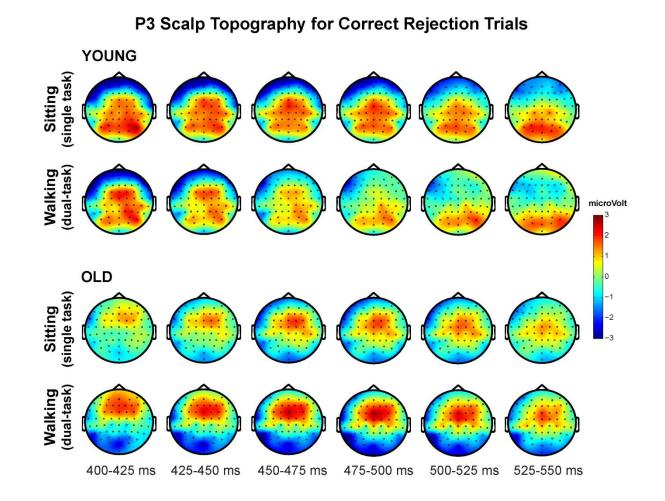


# N2 topographical distribution





# P3 topographical distribution





## Summary

- Younger adults adjust gait and cognitive control when presented with a dual task situation
- Healthy older adults show a lack of flexibility,
  both in terms of adjusting physical behavior and in reconfiguring cognitive control mechanisms at the neural level.

#### Conclusion

- These studies provide highly promising methods for gaining insight into the neurophysiological correlates of self-motion in more naturalistic environmental settings.
- Further our understanding self-motion disorders

## **Overall Conclusion**

- The vestibular system is useful
  - Combines in an optimal fashion with visual cues
  - Is processed like other sensory modalities
- EEG can be collected during active and passive motion
  - With meaning results that further our understanding of self-motion

# Thank you

<u>Albert Einstein College of Medicine</u> Adam Snyder Brenda Malcolm Pierefilipo DeSanctis **John Foxe** 

<u>Trinity College Dublin</u> Hugh Nolan Robert Whelan **Richard Reilly** 

<u>Max Planck Institute for Biological Cybernetics</u> Jennifer Campos **Heinrich Bülthoff** 



Albert Einstein College of Medicine





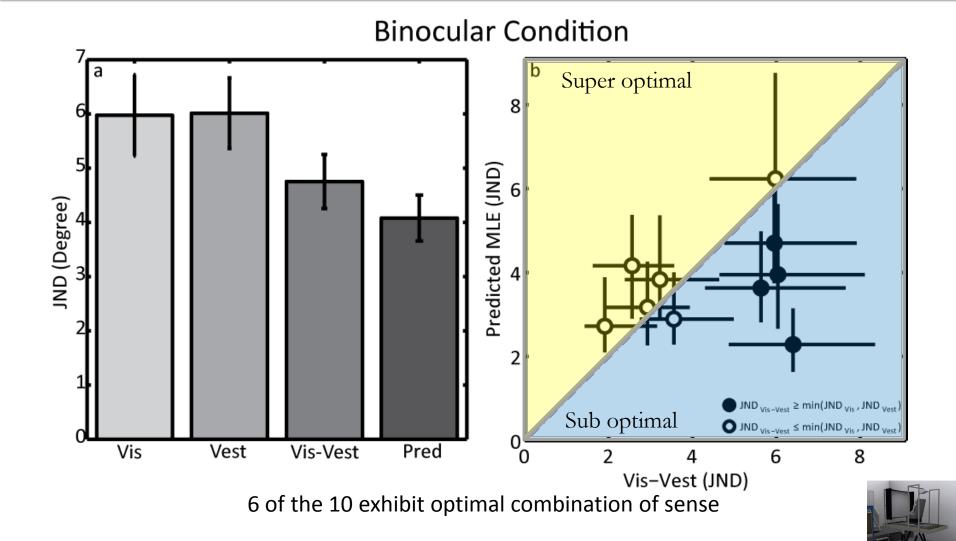
MPI FOR BIOLOGICAL CYBERNETICS

#### Any questions



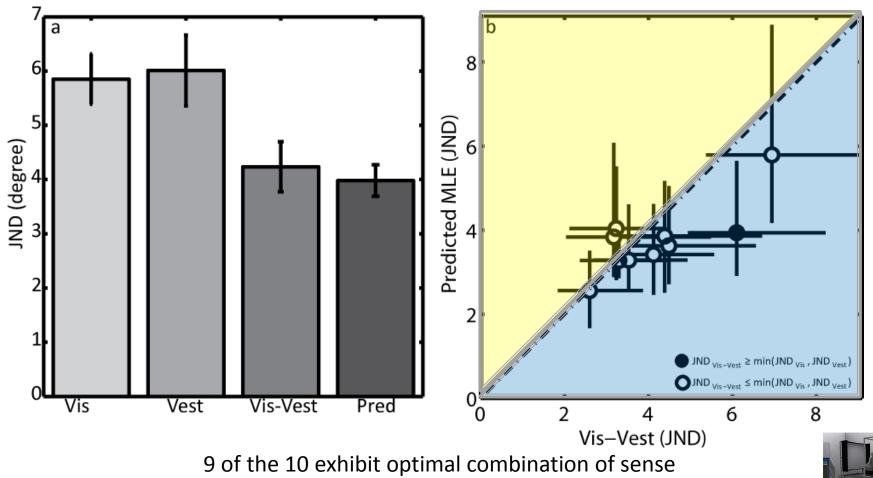


### **Binocular Condition**

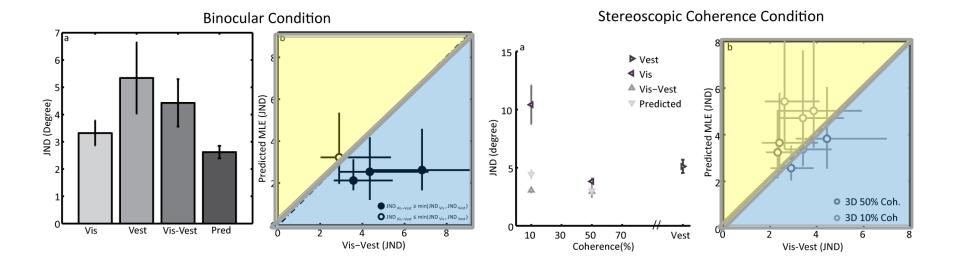


## **Stereoscopic Condition**

Stereoscopic Condition



## Reproducible nature of result



A subset of the original participants were re-run and exhibited identical results

# Summary

- The presence/absence of stereoscopic visual information can impact the extent to which visual and vestibular cues are integrated during heading perception.
  - This was reproducible within participants



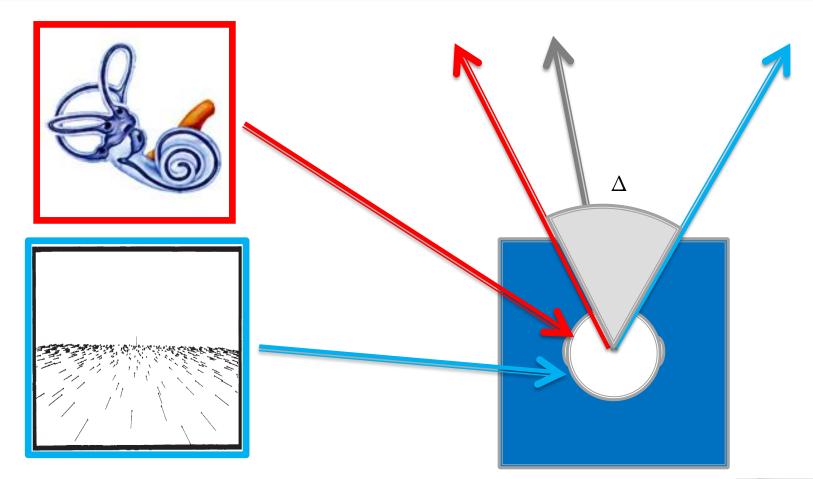
## Talk Overview

#### Passive Heading detection

- 1. The role of Stereo cues
- 2. Conflict of information
- 3. Neural correlates of heading detection change
- Active tasks
  - 4. Walking
  - 5. Neural recordings while walking



Visual-Vestibular Integration for Heading (conflict)





#### Why introduce a conflict?

 By introducing a conflict we can see if there is a breakdown of the combination of sense

• We can calculate the weights given to each cue



# The logic of conflicts

# Equally weighted

#### Vestibular weighted more



Vision weighted more

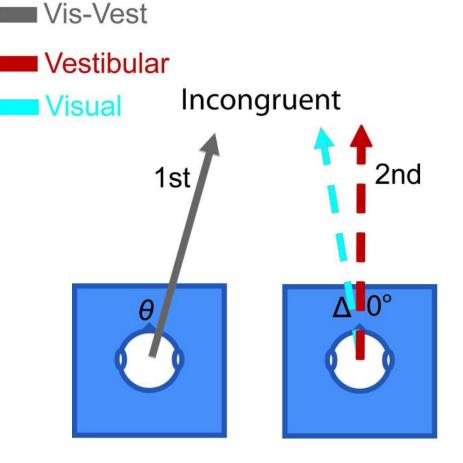


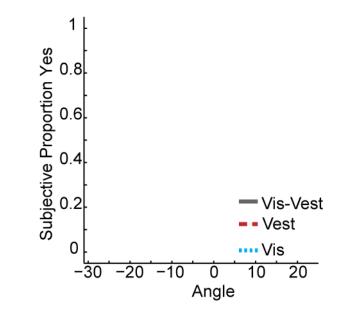




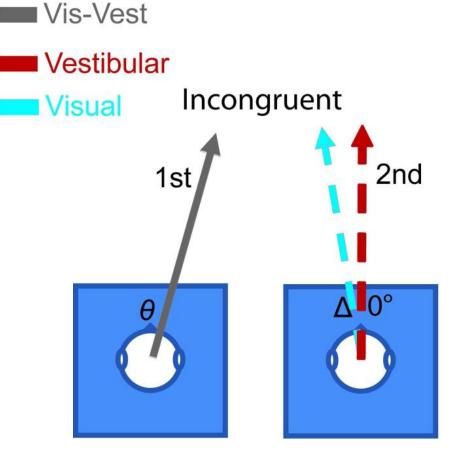


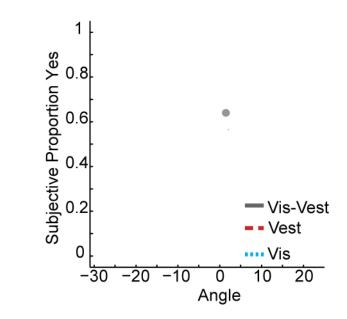




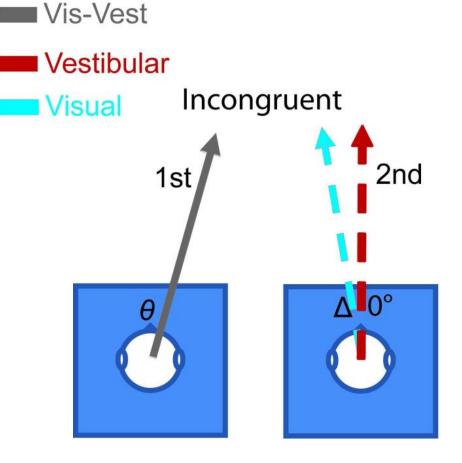


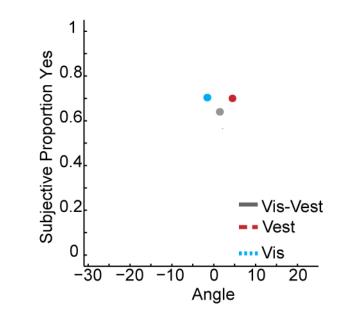




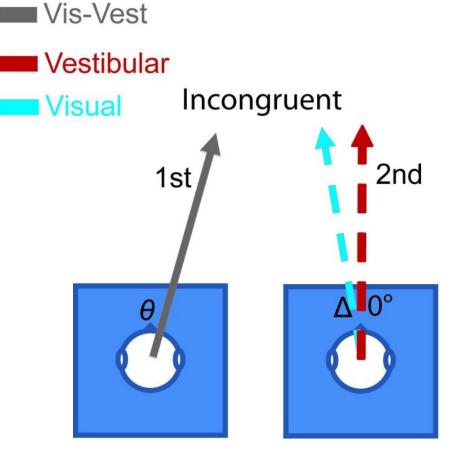


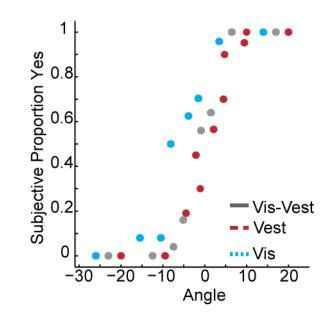




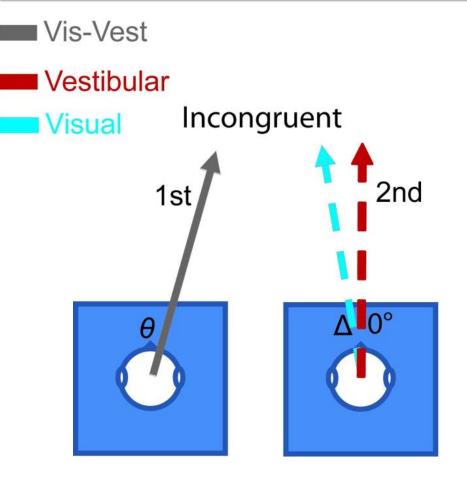






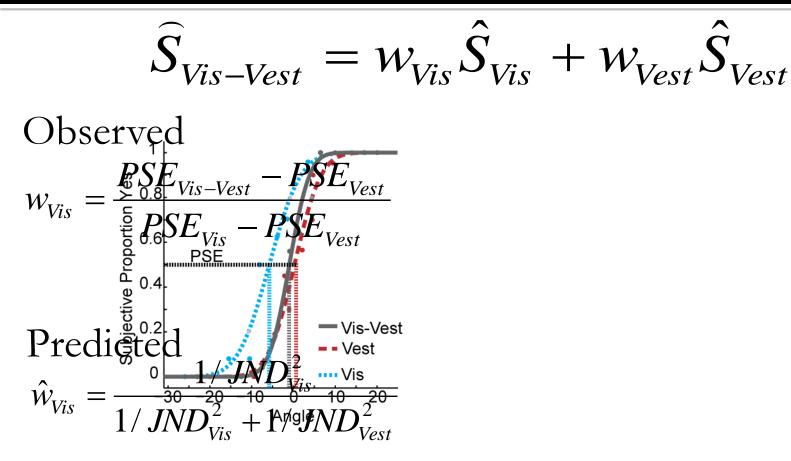








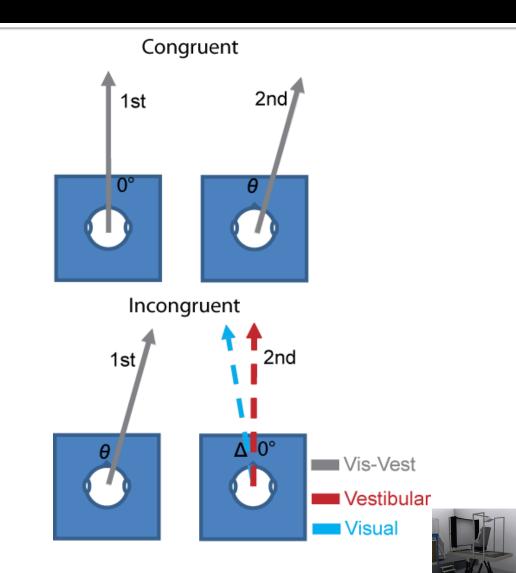
# Maximum Likelihood Estimation



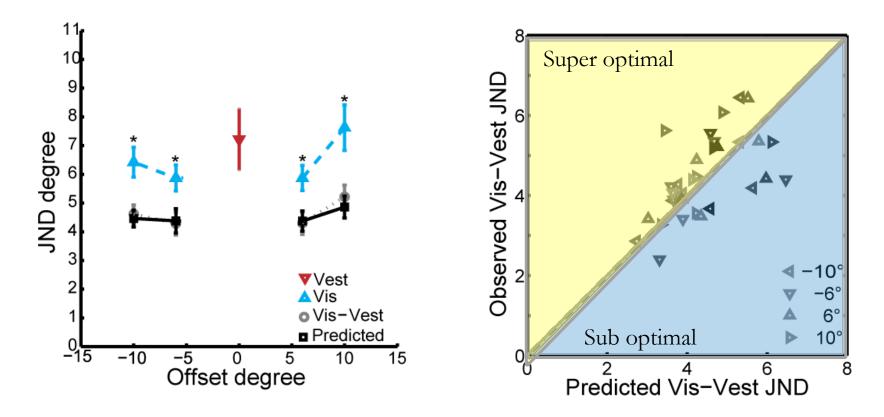


# **Spatial Conflict**

- Conditions
  - 1 Vestibular alone
    - One Standard
    - $\Theta = 0^{\circ}$
  - 4 Visual alone
    - Four standards
    - $\Theta = \pm 6^{\circ}, \pm 10^{\circ}$
  - 4 Visual-vestibular
    - One Standard
    - $\Theta = 0^{\circ}$
    - Four Offset
    - $\Delta = \pm 6^{\circ}, \pm 10^{\circ}$



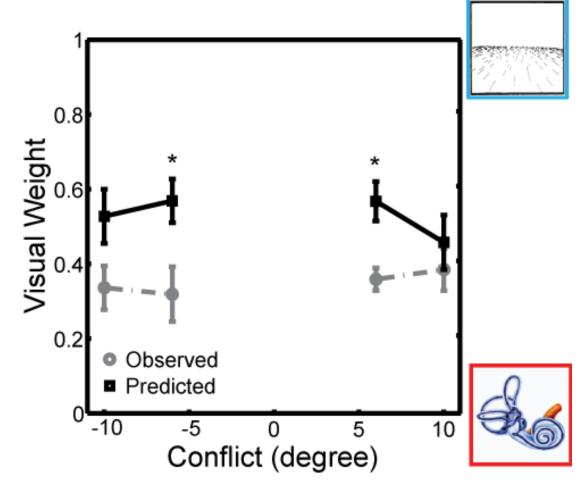
# **Optimal reduction in variance**



The combination of visual and vestibular cues observe an optimal rule of integration







The weights are biased towards the vestibular cue

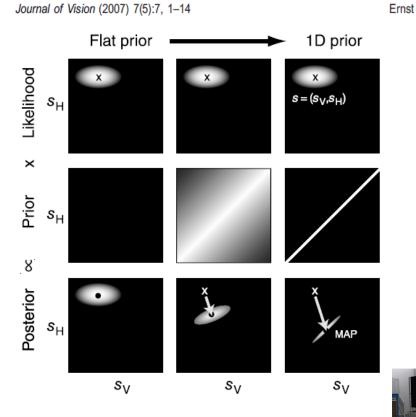


#### Introduction of a Prior

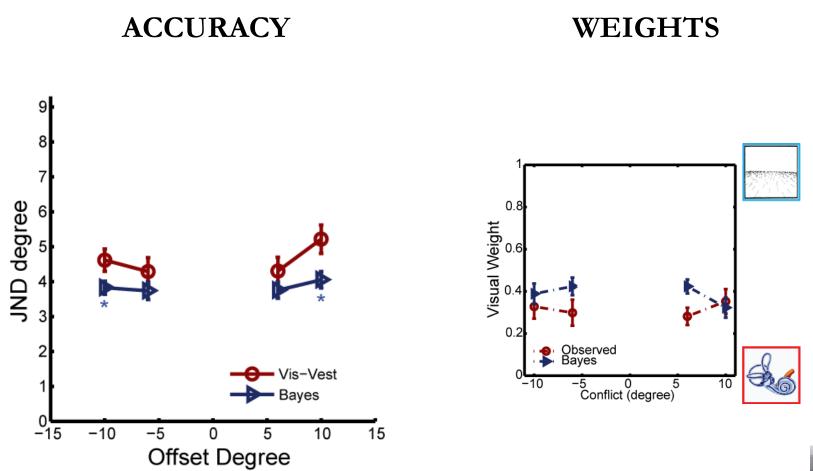
$$\widehat{S}_{Vis-Vest} = w_{Vis} \widehat{S}_{Vis} + w_{Vest} \widehat{S}_{Vest} + w_{Prior} \widehat{S}_{Prior}$$

$$JND_{Vis-Vest}^{2} = \frac{1}{1/JND_{Vis}^{2} + 1/JND_{Vest}^{2} + 1/JND_{Prion}^{2}}$$

$$w_{Vis} = \frac{1/JND_{Vis}^2}{1/JND_{Vis}^2 + 1/JND_{Vest}^2 + 1/JND_{Prior}^2}$$



#### **Bayesian Model**

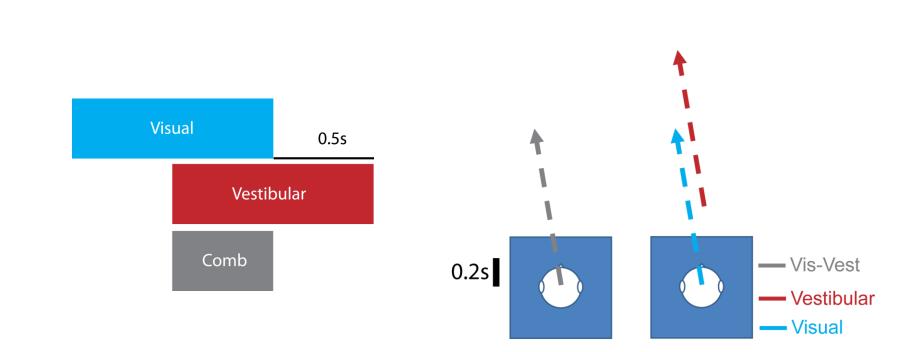


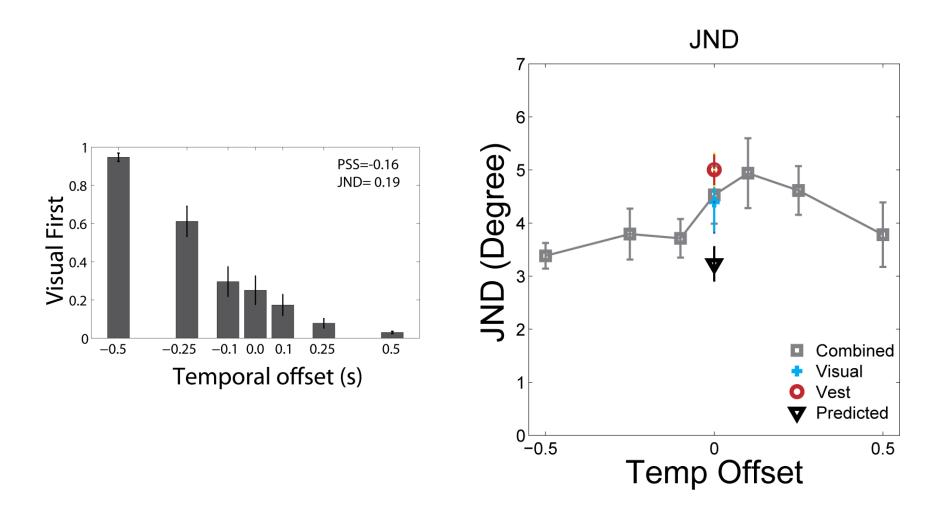
#### Summary results

- Participants exhibited a statistically optimal reduction of variance under combined cue conditions.
- Performances in the unimodal conditions did not predict the weights in the combined cue conditions.
- Therefore, we conclude that visual and vestibular cue combination is not predicted solely by the reliability of each individual cue but rather, there is a prior which leads to a higher weighting of vestibular information in this task.



# **Temporal Conflict**



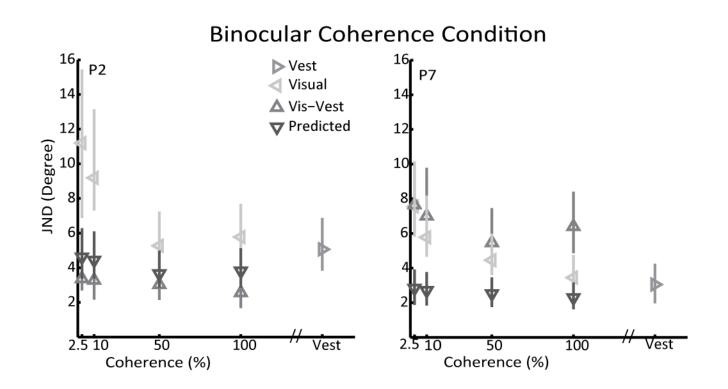


Butler et al (In Prep)

<u>Supplementary</u>

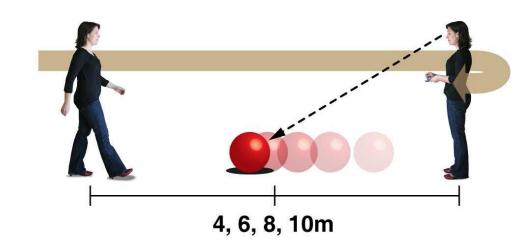


### Reproducible nature of result



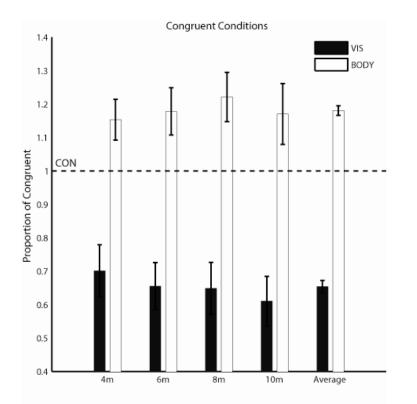
# Multisensory integration in the estimation of walked distances

- Conditions
  - Visual Alone
    - 0.7, 1.0, 1.4
  - Body Cues



- Combined
  - Congruent
  - Incongruent Visual Gain (0.7 1.4)
- 4 distances (4, 6, 8 10m)

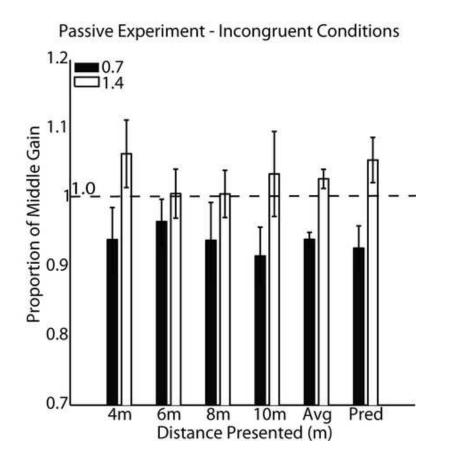
# **Congruent results**



Congruent combined distance estimation sits between visual alone and body based cues



#### **Incongruent Results**



- The combined results are predicted by the unisensory results.
  - Body based we relied upon more than visual cues
- Within body based cues the vestibular cues were relied upon more than proprioceptive cues

Exp Brain Res DOI 10.1007/s00221-012-3048-1 Jennifer L. Campos · John S. Butler · Heinrich H. Bülthoff



#### Conclusion

 The combination of visual and body based cues for walking is predicted by a MLE model

